

# Original Article

## Formulation, release and stability study of Bupropion sustained release 150 mg using Hydroxypropylmethylcellulose (HPMC) 4000cps basis

Open Access

Nafiseh Erfani<sup>1</sup>, Mohamad Reza Avadi<sup>2,3\*</sup>, Assal M.M.Sadeghi<sup>3</sup>, Arash Mahboubi<sup>4</sup>,  
Orkide Ghorban Dadras<sup>5</sup>

1. Department of Pharmaceutics, Pharmaceutical Sciences Branch, Islamic Azad University (IAUPS), Tehran, Iran

2. Department of Nanotechnology, Pharmaceutical Sciences Branch, Islamic Azad University (IAUPS), Tehran, Iran

3. Hakim Pharmaceutical Company, Tehran, Iran

4. Department of Pharmaceutics, school of Pharmacy, Shaheed Beheshti University of Medical Sciences, Tehran, Iran

5. Department of Medicinal Chemistry, Pharmaceutical Sciences Branch, Islamic Azad University (IAUPS), Tehran, Iran

### Abstract

In this study, formulation of sustained-releasing matrix tablet of bupropion 150 mg, using hydroxypropylmethylcellulose (HPMC) 4000cps was evaluated with the aim of reducing the frequency of daily dose. The level of HPMC 4000, polyvinylpyrrolidone (PVP) and magnesium stearate (Mg St) was varied based on a 2 level 3 factor factorial experimental design using the release rate of the drug from the matrices as the response variable. The mechanism of drug release from hydrophilic matrix tablets is complicated but it is known to be related to dissolution of drug and its diffusion through the hydrated portion of matrix and erosion of the outer hydrated polymer on the matrix surface. Granules of the optimum formulations were compressed into tablets using EK-O lorsch single punch tablet machine. Evaluation of tablets including weight variation, crushing strength and friability demonstrated acceptable results. Based on dissolution data of the eight tablet formulations resulted from the experimental design, a polynomial regression equation was generated and used for obtaining the optimum formulations. In vitro dissolution tests also revealed sustained release of drug for an 8 hours period at the end of which almost complete release was achieved. According to release studies formulation A, AB and C has been selected for long term stability studies.

**Key words:** Controlled release, Bupropion, Hydroxypropylmethylcellulose

\*Correspondence to: Dr. Mohamad Reza Avadi, Assistant Prof., Dept. of Pharmaceutics, Pharmaceutical Sciences Branch, Islamic Azad University (IAUPS), Tehran, Iran.

P.O. BOX: 19395-6466

Tel: +98 21 22640051 Fax: +98 21 22602059

Email address: rawwadi@yahoo.com

## 1. Introduction

The hydrophilic matrix tablets designed with water soluble polymers are extensively used in control release development. Among hydrophilic polymers, hydroxypropyl methylcellulose or HPMC is the most widely used excipient due to its distinct advantages: the polymer has an excellent safety record; its non-ionic nature leads to minimization of the interaction problems in acidic, basic, or other electrolytic systems; availability of the polymer in a wide range of viscosity allows for developing different coating formulations and the subsequent screening the most effective ones (Sandi P B. Tiwari, et al; 2008) and finally the data for development studies is abundant. Evidences suggest that HPMC with 4000 cps viscosity is suitable for slowing down drug release especially in shorter period of time (RunnaRao Ravi et al; 2007 and SanatuGhosh et al 2010).

In this study HPMC 4000 was used as sustain release agent for once-daily Bupropion extended-release dosage form. Bupropion is a dopamine –reuptake inhibitor which is used as an antidepressant and prescribed for smoking cessation. The drug however is subjected to some disadvantages including the short biological half-life and high dosing frequency. Studies identified a relationship between peak plasma concentration of bupropion and some adverse effects like epilepsy. These problems render use of the bupropion immediate form inconvenient for patients, and the drug as an important candidate for sustained release development.

Herein we present the report of preparing a suitable extended-release formulation Bupropion. The effect of some factors, such as the concentration of Magnesium Stearate (Mg St) and polyvinyl pyrrolidone (PVP) as well as the concentration of polymer on drug release was investigated by utilizing the 23 factorial designs and the best of formulations were chosen for long term stability studies.

## 2. Materials and Methods

### Materials

The following reagents were used: Bupropion hydrochloride (Supor, India), lactose monohydrate, Microcrystalline cellulose (Avicel), hydroxyl propylmethylcellulose (HPMC), magnesium stearate (Mg St) and polyvinylpyrrolidone were gifts from Hakim pharmaceutical company.

### Equipment

Single punch tablet machine (Lorsch, Germany), U.V. spectrophotometer (Cecil, England), hardness tester (Dr. schleunigerpharmaton 5y, USA), friabilator (Dr. schleunigerpharmaton FR1000, USA), dissolution tester (Erweka DT60, Germany)

### Methods

#### Factorial design experiment:

Tablets were obtained based on the 23 factorial design procedure: HPMC concentration X1; PVP concentration X2; and Mg St concentration X3 were selected as independent variables (table 1) and the effect of these

Table 1: Factors used in the factorial design experiment

Factor	Low level	High level
Hydroxypropylmethylcellulose (%) (X1)	10	15
PVP (%) (X2)	3	5
Magnesium stearate (%) (X3)	1	1.5

variables on drug release was also investigated. The compositions of all model formulation are summarized in (table 2). The percentage of drug release at 1,4,8 were selected (according to

**Table 2: Compositions of the model formulations**

Formulation The formulations(%/tab)	1	A	B	C	AB	AC	BC	ABC	Function of each agent
Bupropion Hydrochloride	60	60	60	60	60	60	60	60	Active Ingredient
HPMC 4000cps	10	15	10	10	15	15	10	15	Retarding Agent
PVPk30	3	5	3	3	5	3	5	5	Binder
AvicelPH102	10	10	10	10	10	10	10	10	Filler
Lactose Monohydrate	16	11	14	15.5	9	10.5	13.5	18.5	Filler
Mg St	1	1	1	1.5	1	1.5	1.5	1.5	Lubricant
Ethanol 96°	0.064	0.064	0.064	0.064	0.064	0.064	0.064	0.064	Solvent for binder

the USP 33) as response variables to detect the profile and ensure complete drug release.

**Tablet preparation:**

The drug and excipients were weighed and mixed well. PVP was dissolved in 96° alcohol and then the solution was added to make a wet mass. Afterwards the wet component was passed through a 14 mesh sieve. The granules were dried in room temperature for 24 hours, and then blended with 1% or 1.5% (dependents on formulation) of magnesium stearate. Tablets containing 150mg of bupropion were compressed using 9 mm diameter concave punches. The upper punch compaction pressure applied was 8-15 kps.

**Evaluation of tablets:**

Tablets were subjected to various physical tests

which include weight variation, thickness, hardness, friability and dissolution testing. For hardness and weight testing, ten randomly chosen tablets were examined from each set. The tablet friability testing was performed on a friabilator. The 10 tablet samples were tumbled for 4 min. Afterwards, the percent weight loss was calculated.

**Determination of the release of bupropion from HPMC 4000cps matrix tablet:**

The United States Pharmacopoeia (33) paddle method was used for all in vitro dissolution studies. Water was used as a dissolution medium. The rate of stirring was 50 rpm. The bupropion tablets were placed in 900 ml of water and maintained at 37°. Five milliliters of samples were taken at appropriate intervals (1,4,8 hrs according to the

USP 33). The samples were analyzed by UV spectrophotometry at 298 nm. At least 3 tablets of each formulation were used. The mean and standard deviation of percentage dissolved were calculated.

Long term stability studie:

Three formulations (A, AB and C) were chosen for long term stability studies which were performed according to the ICH's guideline (temperature:  $25^{\circ}\pm 2$  and moisture:  $60\%\pm 5$ ). The drug release of these three formulated tablets

was studied during 1, 3 and 6 months.

### 3. Result and discussion

Tablets were readily compressed with no change required in the ratio of excipient. The pressed tablets were smooth, shiny and can be applied directly or aqueous polymer coating (for patient more compliance and palatability) in experimental administration. Weight variation was within limit of  $\pm 5\%$ .

Table 3: Physical and chemical parameters of formulated bupropion tablets

factor formulation	thickness	Weight(mg)	Hardness(kp)	(%) friability
	(mm) n=10	N=10	n=10	n=10
1	4.3±0.01	250.2±3.48	9.7 ± 1.02	0.40
A	4.3±0.01	252.3±2.82	11.8±1.22	0.50
B	4.3±0.02	251.4±2.35	11.7±1.71	0.40
C	4.2±0.01	250.7±2.14	11.7±1.48	0.10
AB	4.1±0.01	250.3±2.10	13.5±1.75	0.30
AC	4.2±0.01	249.1±1.58	11.5±0.93	0.52
BC	4.2±0.01	251.9±1.67	9.7±0.91	0.40
ABC	4.2±0.01	250.9±2.15	10.6±1.51	0.56

The hardness was set at 8 to 15 kps. Table 3 represents the actual values. Thickness was set at a range of 4.2 mm  $\pm$  5%. Mean drug content value obtained by assay

procedure was within the USP's range (90% to 110%). The dissolution profiles and the responses of all model formulations required by the

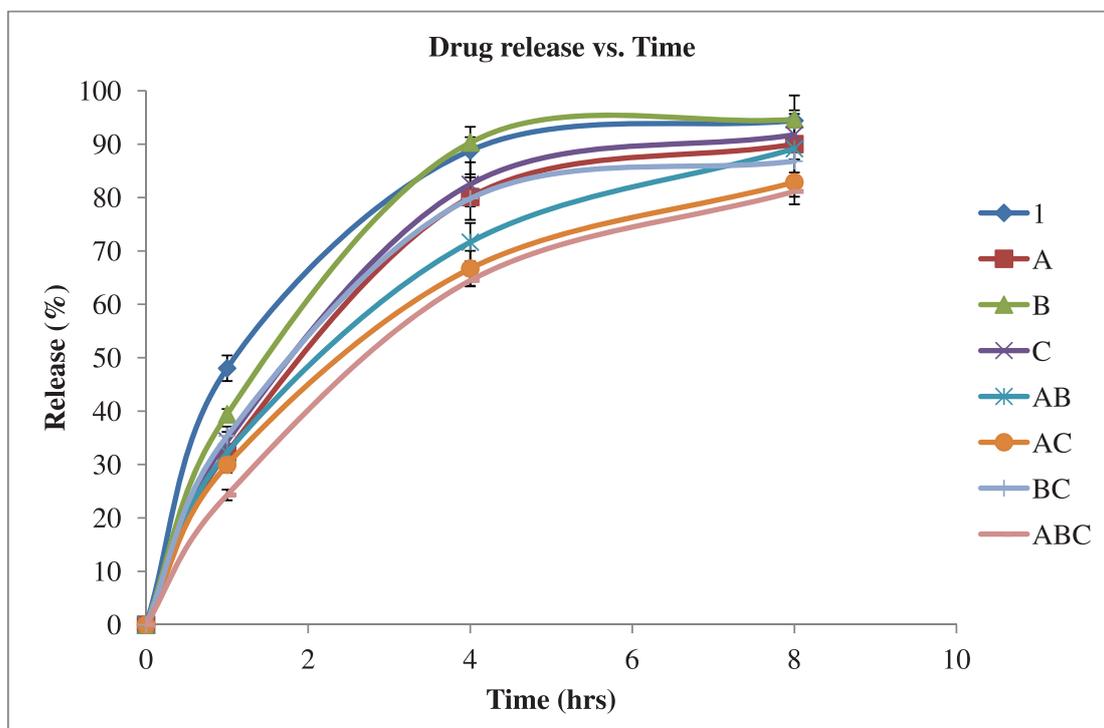


Figure 1: Drug release profile of Bupropion in different formulations of sustained release tablets

factorial design are given in Fig. 1 and Table 4 respectively. The wide variation indicates the different drug release rates as a result of combinatorial factor effects. Table 4 indicates that variables at low compared to high levels show significant changes in drug

release. In formulation 1 which all variables are at low level drug release is higher than the range defined by USP 33. On the other hand, in formulation ABC which all variables are at high level drug release is lower than USP range. So it can be concluded that the selected

Table 4: Drug release from different formulations in defined intervals

Release (%) / Time(hr)	I	A	B	C	AB	AC	BC	ABC
1	48.3 $\pm$ 0.66	32.2 $\pm$ 0.78	39.4 $\pm$ 0.71	34.4 $\pm$ 0.81	32.2 $\pm$ 0.72	29.9 $\pm$ 0.65	35.3 $\pm$ 2.7	24.3 $\pm$ 0.66
4	88.8 $\pm$ 0.67	80.1 $\pm$ 0.75	90.3 $\pm$ 0.73	82.5 $\pm$ 0.77	71.6 $\pm$ 0.75	66.6 $\pm$ 0.70	79.8 $\pm$ 0.3	64.4 $\pm$ 0.70
8	94.4 $\pm$ 0.7	90.0 $\pm$ 0.77	94.6 $\pm$ 0.77	91.7 $\pm$ 0.79	89.1 $\pm$ 0.7	82.8 $\pm$ 0.68	86.8 $\pm$ 1.4	81.1 $\pm$ 0.69

range is a suitable range and by evaluating these result a formulation with suitable physical and chemical features as well as drug release can be selected.

By reviewing the drug profile, it can be explained that the rate of drug release as well as the burst effect decreased with an increase in the tablet content of HPMC4000 cps. Moreover drug release in formulation A (with HPMC at high level) is lower than drug release in formulations 1, B and C suggesting that at high levels of HPMC the release of drug will be reduce significantly comparing to Mg St and PVP.

For the controlled release under investigation, which is a matrix-tablet comprising drug, and hydrophilic polymer (HPMC), the release should follow three steps.

First the dissolution medium is penetrated in the tablet matrix (hydration). Then the matrix is swelled with concomitant dissolved. The dissolved drug is finally transported either through the hydrated matrix or from the parts of the eroded tablet, to the surrounding dissolution medium (Kiorstis, Kachrimanis et al. 2005).

The obtained release profiles, suggest that high levels of PVP has small affect on reduction of drug release. The drug release of the formulation B is almost similar to that of formulation 1. Although the release profile in formulation B is marginally lower than formulation 1. Therefore, PVP in high concentration could have positive effect on reduction of drug release. This is perhaps due to an increase in bonds and reduction of water penetration into system, consequently water absorption by HPMC polymer and create gel layer will decrease, that could inhibit drug release. Comparison of (what of) formulations (B) (with high level of PVP) and C (high level of Mg St), shows that Mg St has stronger effect on decreases drug release relative to PVP which can be explained by the hydrophobic nature of Mg St: once the tablet is exposed to water or gastro intestinal fluid, less water may enter to the tablet and absorbed by

HPMC polymer resulting in a decrease matrix swelling and a slow drug release.

By studying the profile, it is revealed that even though high levels of PVP cannot have significant effect on drug release but sufficiently high levels of both PVP and Mg St (corresponding to formulation BC) may cause a slowdown in the release of the drug. As a result PVP at high level and Mg St at high level could prevent water penetration and delay the formation of a gel layer by HPMC polymer and the swelling mechanism to further slow down the drug release. By comparing formulation BC (PVP and Mg St at high level) with formulation AB (PVP and HPMC at high level) it can be concluded that PVP and HPMC at high level is more effective in alleviation of the drug release comparing to PVP and Mg St at high level. This indicates that HPMC is the main factor in sustain releasing the drug.

Also when Mg St and HPMC at high level are used, drug release shows more reduction compared to PVP and HPMC at high levels. This confirm that Mg St has a greater effect on sustain releasing the drug in comparison to PVP.

The drug release of the three formulations 1, ABC and B is out of the range defined by USP 33, therefore, they were rejected. Among the five remaining formulations, although the drug release in formulations BC and AC were in the USP defined range, less drug was released especially at the last time (after eight hours). Although the reduction of drug release was the main goal in this study but sufficient drug has to be released in predetermined time comparable to the gastrointestinal residence time. Therefore the formulations were not selected for stability studies and instead the three formulations (A), (AB) and (C) which release appropriate amount of drug were used for further stability studies.

In long term stability studies, none of the formulated tablets showed any change of color, smell or physical appearance. Moreover the release of drugs in all three formulated drugs

Table 5: Drug release studies after 6 month of long term stability

Release(%) Time(hr)	A	AB	C
0	0	0	0
1	33.51±0.66	31.90±0.70	34.23±0.58
4	81.76±0.62	77.92±0.68	83.37±0.60
8	99.71±0.69	98.01±0.67	102.0±0.55

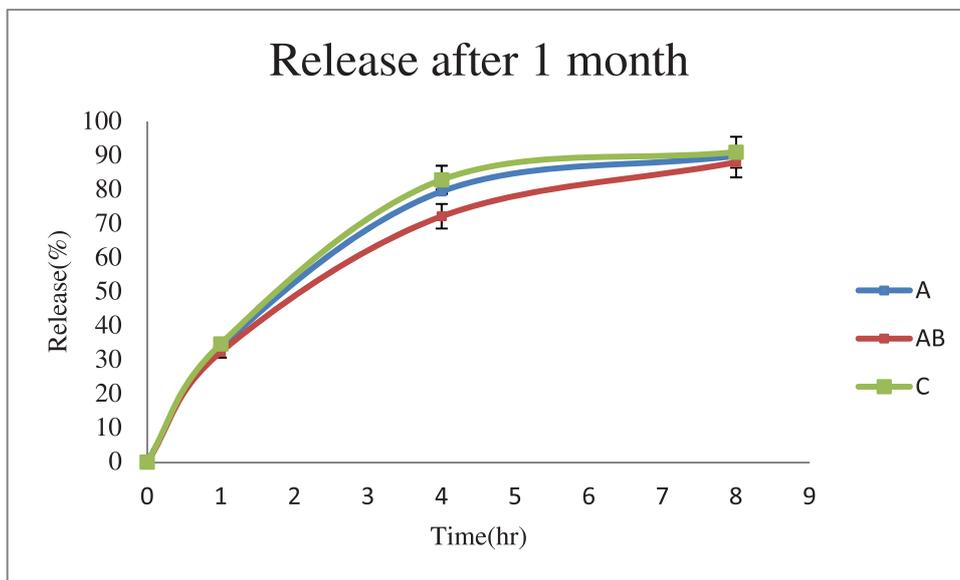


Figure 2: Drug release profile of Bupropion sustained release tablets after 1 month

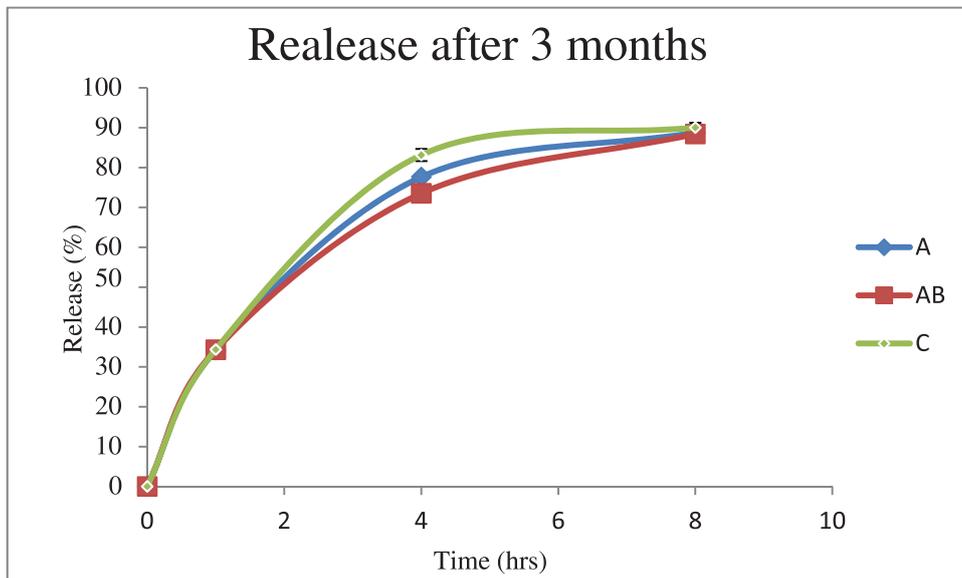


Figure 3. Drug release profile of Bupropion sustained release tablets after 3 month

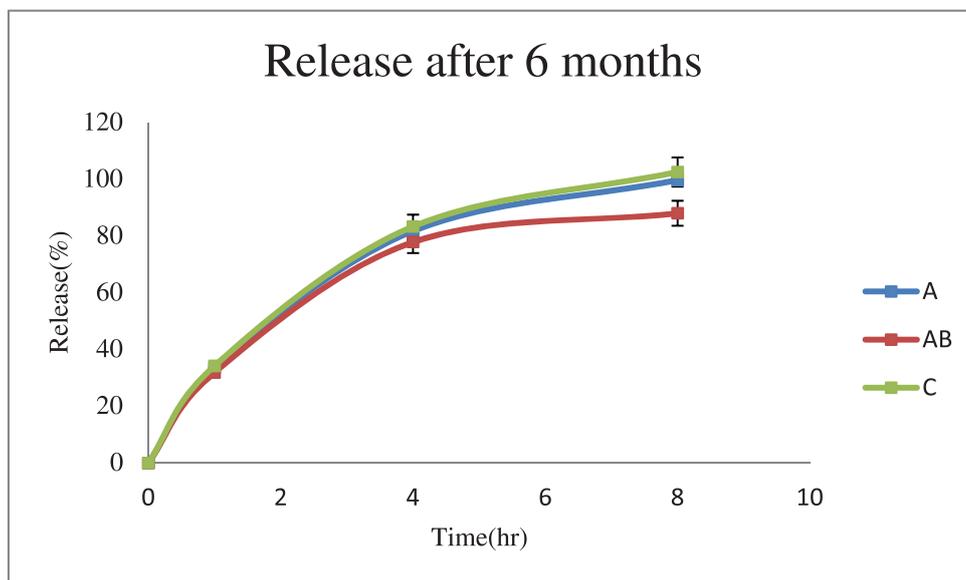


Figure 4: Drug release profile of Bupropion sustained release tablets after 6 months

in months 1,3 and 6 were validated according to the USP 33 instruction

#### 4. Conclusion

Bupropion sustained release matrix tablet was prepared successfully using HPMC 4000cps polymer by a 23 factorial design to retard the drug release and achieve an optimum dissolution profile. The results of this study showed that HPMC was the main determining factor. Also Mg St had more effect on sustain releasing the tablet than PVP.

#### 5. Acknowledgment

The help and cooperation of Hakim Pharmaceutical Company's R&D is greatly appreciated.  
**Conflict of interests** : None declared.

#### 6. References

A. Nokhodchi, S. Norouzi-Sani, M.R. Siahi-Shadbad, M. Lotfipoor, The effect of various surfactants on the release rate of propranolol hydrochloride from hydroxypropylmethylcellulose (HPMC)—Eudragit matrix, *Eur. J. Pharm. Sci.* 2002;54: 349–356.

Charles F.Lacy, Lara L.Armstrong, Morton P.Goldman. Drug information handbook. 18th ed. American Pharmacists Association; 2009-2010.p.238.

E. Lahdenpaa, M. Niskanen, J. Yliruusi, Crushing strength disintegration time and weight variation of tablets compressed from three MCC pH grades and their mixtures, *Eur. J. Pharm. Biopharm.* 1997;42: 315–322.

J.Z. Li, G.S. Rekhi, L.L. Augsburger, R.F. Shangraw, The role of intra- and extragranular microcrystalline cellulose in tablet dissolution, *Pharm. Dev. Tech.* 1996;1: 343–355.

Kiortsis S, Kachrimanis K, Broussali Th and Malamataris S. Drug release from tableted wet granulations comprising cellulosic (HPMC or HPC) and hydrophobic component. *Eur. J. Pharm. Biopharm.* 2005; 59: 73-83.

L.C. Feely, S.S. Davis, Influence of surfactants on the drug release from hydroxypropylmethylcellulose, *Int. J. Pharm.* 1988; 41: 83–90.

M. Vlachou, N. Hani, M. Efentakis, P.A. Tarantili, A.G. Andreopoulos, Polymers for use in controlled release system: the effect of surfactants on their swelling properties, *J. Biomater. Appl.* 2000;15:65–77.

N.D. Eddington, M. Ashraf, L.L. Augsburger, J.L. Leslie, M.J. Fossler, L.J. Lesko, V.P. Shah, G.S. Rekhi, Identification of formulation and manufacturing variables that influence in vitro dissolution and in vivo bioavailability of propranolol hydrochloride tablets, *Pharm. Dev. Tech.* 1998;3: 535–547.

N .Katori, K. Okudaria, N. Aoyagi, Y. Takeda, M. Uchiyama, In vitro and in vivo correlation for controlled-release formulation of chlorpheniramine maleate, *J. Pharmacobiodyn.* 1991;14:567–575.

Punna Rao Ravi, Sindhura Gonga, Ranendra Narayan Saha. Design and study of Lamivudine oral controlled release tablets. *AAPS Pharm Science.* 2007;8(4):167-175.

Sanatu Ghosh, B B Barik. Formulation and in vitro evaluation of once daily sustained release formulation of Aceclofenac. *J Pharm Res.* 2010;9(3):265-273.

Sandi P B. Tiwari, [et al]. Modulation of drug release from hydrophilic matrices. Advancing process solutions Pharmaceutical Technology, extended release improving formulation of HPMC matrices. 2008

T. Uchida, M. Kawata, S. Goto, In vivo evaluation of ethyl cellulose microcapsules containing ampicillin using rabbits, dogs and humans, *J. Pharmacobio-Dyn.* 1986;9 : 631–637.

W. Cressman, D. Summer, The dog as a quantitative model for evaluation of non-disintegrating sustained-release tablets, *J. Pharm. Sci.* 1971;60 :132–134.

Yaw Bin Haung, Tsai Yi-Hung, Yang Wan-Chieh, Chang Jui-Sheng, Pa-Chu Wu, Kozo Takayama. Once daily propranolol extended release tablet dosage form formulation design and in vitro/in vivo investigation. *Eur J Pharm Biopharm.* 2004;58:607-614.